## Section 28: Bone Plate Analysis and Design

# Biomechanics of Bone Fx

- Weakest in Tension, Strongest in Compression
- Pure **Bending → Transverse**Fx
- **Torsion** Æ **Spiral** Fx
- Shear → Oblique Fx
- **Butterfly** due to **Bend <sup>+</sup> Shear**



# Screw fixation

- Rotary forces  $\rightarrow$  compression between objects (inclined plane on spiral pulls object toward head)
- Four part construction: *head, shaft, thread, tip*
- Thread defined by *root diameter, thread di t it h diame ter, pitc*

#### **Screws**

- *Larger core* diameter has *higher resistance to fatigue & shear failure*
	- 4th power of the diameter
- **Pullout strength** (maximum force screw can support along its axis)
	- –– outer diameter, length of engagement, shear strength/density of bone



## Screw fixation



28-5 From: Justice

# Interfragmentary compression screw

- Lag screw can convert *torque forces* to <sup>a</sup> *compressive force*
- Screw should be *perpendicular* to fracture preventing sliding of fragments when compressed
- *Gliding hole* => cortex under screw head drilled to thread diameter
- *Thread hole* => opposite glide hole; drilled to the core diameter of screw





28-7 From: Justice

## Interfragmentary compression screw

• This alone is well suited for avulsion, epiphyseal, metaphyseal and intraarticular fractures- absolute stability, no callus



28-8 From: Justice

## Plate and screw fixation

- For transverse or short oblique fx, screws must be combined with other internal fixation
- Principle based on converting *tension force* to *compression force*
- Accomplished by placing plate on *tension* or *convex* side of bone

#### Plate and screw fixation



<sup>28-10</sup> From: Justice

## Plate and screw fixation

- Plates offer benefits of **anatomic** *reduction* and stability for early motion, but must be *protected from early weight bearing.*
- Ideall y *3 -4 screws* on each side of fracture
- Prebending the plate to increase compression

- $\bullet\,$  Function of the plate
	- –Internal splint
	- Com pression
- "The bone protects the plate"



- •• Fracture Gap / Comminution | Applied Load
	- – Allows bending of plate with applied loads
	- Fatigue failure



# Plates & Bending failure

- Leaving gap opposite plate makes it a fulcrum
- increased stress at holes
- avoid holes over fracture sites
- • greater the span between screws
	- less stiff
	- more bending





- Bone-Screw-PlateRelationship
	- –Bone via compression
	- –Plate via bone-plate
	- $\rightarrow$ **Friction**
	- Screw via resistance **to bending and pull** out.



- Plates:
	- Bendin g stiffness **Hei ght g** proportional to the thickness (h) of the plate to the 3 d **Base (b) (h)** the plate to the  $3^{\mathsf{r}}$ power. **I= bh3/12**

- $\bullet\,$  The screws closest to the fracture see the most forces.
- The construct rigidity decreases as the distance between the innermost screws increases.



• Number of screws (cortices) recommended on each side of the fracture:



## Prebending





28-19 From: Justice



28-20 From: Justice

• Tension Band Plate



#### Fig. 3.2.2-23: Tension band principle at the femur.

The intact femur (a) is an eccentrically loaded bone with distraction or tensile forces laterally and compression on the medial side. In case of a fracture (b) the lateral fracture gap will open, whereas the medial will be compressed. If a plate is placed alongside the linea aspera of the femur (c), it will be under tension when loaded, thereby compressing the fracture gap, provided there is bony contact medially. If the plate is placed to the compression side (d), it is not able to prevent opening of the lateral gap (instability). If the medial cortex is not intact (e), the tension band principle cannot work, because of lack of buttress (see chapter 3.2.3).